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ORIGINAL RESEARCH

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Preclinical validation of occupational and environmental safety of an isolation system for noninvasive ventilation in COVID-19 and other aerosol-transmitted infections

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ABSTRACT

Background: The current SARS-CoV-2 pandemic has provoked the collapse of some health systems due to insufficient intensive care unit capacity. The use of continuous positive airway pressure (CPAP) and high-flow nasal oxygen (HFNO) therapies has been limited in consideration of the risk of occupational infection in health-care professionals.

Aims: In preclinical experimental simulations, evaluate occupational and environmental safety of the newly developed isolation system for aerosol-transmitted infections (ISATI).

Method: Simulations were conducted to test ISATI's capability to isolate aerosolized molecular (caffeine), and biological (SARS-CoV-2 synthetic RNA) markers. Caffeine deposition was analyzed on nitrocellulose sensor discs by proton nuclear magnetic resonance spectroscopy. Synthetic SARS-CoV-2 detection was performed by reverse transcription-polymerase chain reaction.

Results: ISATI demonstrated efficacy in isolating molecular and biological markers within the enclosed environment in simulated conditions of CPAP, HFNO and mechanical ventilation therapy. Neither the molecular marker nor substantial amounts of synthetic SARS-CoV-2 RNA were detected in the surrounding environment, outside ISATI, indicating appropriate occupational safety for health-care professionals. **Conclusion**: Aerosolized markers were successfully contained within ISATI in all experimental simulations, offering occupational and environmental protection against the dissemination of aerosolized microparticles under CPAP or HFNO therapy conditions, which are indicated for patients with acute respiratory infections.

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1. Introduction

Respiratory viruses can be highly infectious, mainly due to person-to-person transmission through respiratory droplets produced by expiration, coughing, or sneezing [1]. Infected individuals present a range of clinical manifestations, from flulike symptoms to severe pneumonia, in some cases necessitating oxygen support and/or hospitalization [1,2]. Reports of viral aerosol transmission, notably in hospital environments, presents a challenge to the occupational safety of health professionals [1,3–5]. In the SARS-CoV-1 outbreak in Canada in 2003, half of all cases resulted from the nosocomial contamination of health professionals [6]. Studies indicate that coronavirus particles can remain viable in external environments for hours, supporting the notion of high rates of incidence with regard to occupational contamination [7–9].

As health-care professionals face a greater risk of transmission during aerosol-generating procedures performed in patients infected with respiratory viruses, strict requirements have been implemented with regard to the use of noninvasive ventilation (NIV), continuous positive airway pressure (CPAP) and high-flow nasal oxygen (HFNO) therapies [5,6,10–12]. The isolation of rooms by laminar airflow and negative pressure has made the widespread use of NIV and HFNO infeasible in the face of the COVID-19 pandemic [6,10–12]. In an effort to avoid hospital airflow system contamination by aerosolized viral particles generated when performing HFNO and CPAP therapies, these procedures are often not performed even when indicated [6,10–12].

The COVID-19 pandemic has demonstrated the capacity of respiratory viruses to collapse health-care systems worldwide [11,13]. COVID-19 patients who progress to respiratory failure, necessitating orotracheal intubation and prolonged periods of mechanical ventilation during hospitalization, have placed high demands on intensive care units (ICU) [6,11,13]. Treatment guidelines designed to limit aerosol transmission by COVID-19 patients have recommended early orotracheal intubation with mechanical ventilation, further exacerbating

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pressure on hospital ICUs [6]. In several countries, baseline ICU bed capacity has been exceeded [11,13]. In this scenario, emergency temporary measures, including treating hypoxemic COVID-19 patients with CPAP or HFNO, were not possible due to occupational contamination risk, despite these oxygen support therapies being appropriate therapeutic alternatives for affected patients [6,10,14,15].

This manuscript describes preclinical experiments for validation of an easily implementable system for the isolation of patients with respiratory virus infection, denominated Isolation System for Aerosol-Transmitted Infections (ISATI). The objective is to safely enable an alternative for oxygen delivery via NIV or HFNO for patients with mild or moderate hypoxemia, especially in hospital environments challenged by infectious aerosol transmission with deficient ICU capacity. ISATI has been designed to prevent viral contamination in hospital environments, and thus increase the occupational protection of health professionals and other hospitalized patients. The present report aims to evaluate the effectiveness of the proposed system in retraining the dissemination of aerosolized molecular and biological markers in simulated CPAP, HFNO and mechanical ventilation procedures.

2. Methods

2.1. Description of the isolation system for aerosol-transmitted infections (ISATI)

ISATI possesses two distinct security features: a physical barrier between the patient and the external environment, and a microparticle filter for connection to hospital vacuum pump systems. The physical barrier consists of a transparent polyethylene plastic cover (measuring 5x4x0.001 m) manufactured by Bhiosupply®. To maintain the plastic cover elevated over the patient, a sterilizable, stainless steel structure was designed (Bhiosupply®), which allows the system to dynamically adapt to any type of hospital bed and also enables the hospital bed to be fully elevated. The sizable plastic cover surrounds the entire hospital bed and is fixed to the inferior part of the bed via a polyester and elastane elastic band (Figure 1). A 0.1-0.2µ porous membrane microparticle filter (Bhiosupply®) enables connection to a hospital vacuum pump system or can be connected to another vacuum pump at a suction pressure outflow rate of 40 L/ min. The air suction system connected to the microparticle filter aspirates continuously the air under the plastic cover. The disposable components of ISATI are the plastic cover and microparticle filter. Non-disposable autoclavable components are fabricated from stainless steel.

2.2. Molecular marker analysis by proton nuclear magnetic resonance spectroscopy

Chemical monitoring (internal and external) was performed using strategically positioned pairs of nitrocellulose discs (NC 47 mm 8.0 μ) used as sensors to detect the molecular marker (Figure 2), caffeine (1,3,7-trimethylpurine-2,6-dione), which was dispersed (1% w/v solution) within the ISATI via either pressurized aerosolization or nebulization. The air suction system under the plastic cover was activated during all experiments. Upon conclusion of each experiment, all sensor discs were removed and placed inside 5 mL Eppendorf tubes protected from light for posterior analysis.

All sensor discs were sonicated in their respective Eppendorf flasks for 5 minutes in a 0.6 mL D_2O solution containing 0.2% TSP-d4 [3-(trimethylsilyl) propionate-2,2,3,3 -d4





Figure 2. Positioning of nitrocellulose sensor discs. Position 1: entrance of multiparameter patient monitoring cables and respiratory tubes; position 2: entrance of intravenous therapy tube; position 3: on a health professional's chest; position 4: inside the ISATI.

sodium]. The extracted solution was then analyzed by proton nuclear magnetic resonance spectroscopy (¹H-NMR).

All ¹H-NMR analysis was performed using a 14.1 T (600 MHz for hydrogen frequency) Bruker AVANCE III HD 600 MHz nuclear magnetic resonance spectrometer, using a 5 mm proton-optimized triple cryo-probe, with the sampling temperature maintained at 298 K during the entire analysis using a pulse sequence with a continuous wave pre-saturation and gradient field. The following acquisition parameters were utilized: acquisition time (AQ = 4.18 s), relaxation delay (d1 = 1 s), spectral width (SWH = 7837 Hz), number of scans (ns = 128), received gain (rg = 128) and pulse duration (p1 = 7.7 μ s). The obtained readings were processed using TopSpin® software (Bruker version 3.5 pl7) without apodization. For detection limit determination of 1 ppm, a water 1% caffeine solution was used, using identical acquisition and processing conditions as described above.

2.3. Production of synthetic SARS-CoV-2 RNA and reverse transcription polymerase chain reaction amplification

Sequences of the amplification sites of SARS-CoV-2 genes E, RdRp and N, along with the T7 promoter sequence, were synthetized as duplex DNA oligonucleotides; in vitro transcription was performed using a T7 RiboMAX[™] Express Large Scale RNA Production System (Promega, Madison, WI, USA) in accordance with the manufacturer's instructions. The generated synthetic RNA transcripts were mixed in 15 mL of 0.9% NaCL solution at the following concentrations: 10^{10} RNA copies/mL for the E gene and 10^7 RNA copies/mL for genes N and RdRp. Detection was performed by reverse transcription-polymerase chain reaction (RT-PCR) using a commercially available multiplex kit (AllplexTM 2019-nCoV Assay – Seegene, Seoul, South Korea), following the manufacturer's instructions. RT-PCR was performed on a 7500 Fast Real-Time PCR system (ThermoFisher Scientific, Waltham, MA, USA) using a total of 45 amplification cycles for each tested sample. Amplification of the nucleic acid was detected by accumulation of a fluorescent signal, giving a cycle threshold (Ct) value, which is inversely proportional to the amount of target nucleic acid in the sample.

2.4. NIV with CPAP simulation

In all experimental simulations, an Airway Management Trainer manikin (Laerdal[®]) was placed on a hospital bed inside the ISATI enclosure. To simulate hypoxic conditions associated with respiratory viruses, a tube was attached to the manikin to simulate intravenous therapy, in addition to multiparameter patient monitoring cables and respirator tubes. CPAP was performed using an orofacial mask set at a continuous positive pressure of 15 cm H₂0, programmed to 14 breaths/minute. In the two initial CPAP simulations, 15 mL of caffeine solution (1% in D₂O) was sprayed inside the ISATI using a BhioQap[®] spraying device under high-pressure aerosolization (average pressure of 200 psi) at

a flow rate of 2 mL/s for a period of 90 minutes. A vacuum pump was activated to remove air from inside the ISATI at flow rate of 40 L/min throughout the duration of the experiment. In a third CPAP simulation scenario, 15 mL of caffeine solution was aerosolized using a medical nebulizer, with the hospital's vacuum pump system again used to remove air from inside the ISATI. In a fourth CPAP experiment, a 15 mL suspension of 0.9% NaCL containing 10¹⁰ RNA copies/mL of the E gene, as well as 10⁷ RNA copies/mL of N and RdRp genes, was sprayed inside the ISATI using a nebulizer with internal suction maintained via the hospital's vacuum pump system for 60 minutes. Samples were collected using swabs inside and outside the ISATI for RT-PCR analysis; three samples were collected for each position used for the sensor disks used to detect the molecular marker. Importantly, sensors for molecular marker identification were only removed, and samples for RT-PCR analysis were only collected, including those on the health professional's chest (Figure 2), following the complete disassembly of the ISATI, including disposal of the plastic cover and all disposable items.

2.5. HFNO simulation

To simulate HFNO, the same experimental setting was established as described above. A nasal cannula was positioned in the airway of the manikin (Laerdal®) with an oxygen flow setting of 80 L/minute. A nebulizer was used to spray 15 mL of a 0.9% NaCL solution containing 10¹⁰ RNA copies/ml of the E gene, in addition to 10⁷ RNA copies/mL of genes N and RdRp, inside the ISATI, with air suction via a hospital vacuum pump system maintained during the entire 60-min experimental period. Samples were collected from inside and outside the ISATI for RT-PCR analysis at the same positions as described for NIV with CPAP simulation. Samples for RT-PCR analysis were only collected, including those on the health professional's chest (Figure 2), following the complete disassembly of the ISATI, including disposal of the plastic cover and all disposable items.

2.6. Mechanical ventilation simulation

The ISATI was assembled using the same configuration described in the previous sections. Over a 6-h period, three aerosolizations, at 120-min intervals, of 10 mL of the 1% caffeine solution were achieved using a pump delivering 200 psi of pressure (BhioQap®) at a flow rate of 2 mL/s. Again airflow exhaust was performed by connecting the ISATI to the hospital vacuum pump system at a flow rate of 40 L/min. Another simulation conducted over a 6-hour period was performed using continuous nebulization while connected to the hospital vacuum pump system. In both experiments, nitrocellulose sensor discs were collected every 2 h. At the end of the 6-h period, sensors for molecular marker identification were only removed, including those on the health professional's chest (Figure 2), following the complete disassembly of the ISATI, including disposal of the plastic cover and all disposable items.

3. Results

Similar results were obtained using high pressure aerosolization (average pressure of 200 psi) versus aerosolization with a nebulizer. In both simulation scenarios, the internal environment of the ISATI was saturated with droplets. ISATI's internal air suction method, when connected to hospital's vacuum system or using a pump machine with suction pressure of 40 L/min, did not interfere in the results. No traces of the molecular marker were detected on any of the sensor discs positioned outside the ISATI.

The standard ¹H-NMR spectra analysis of the caffeine solution, depicting a typical signature for this molecule, is shown in Figure 3, Spectrum A. The chemical shifts (δ) of the methyl groups (δ = 3.28; 3.45; 3.91 ppm) and of the purine hydrogen (δ 7.88 ppm) are evident. A similar pattern is observed in spectrum D (yellow line), which corresponds to the sensor discs positioned inside the ISATI (positive control sensors) (Figure 2, position 4) during the NIV with CPAP simulation. However, this signature is not evidenced in either spectrum B, the sensor disc positioned at the entrance of the patient monitoring cables and respiratory tubes (Figure 2, position 1), or spectrum C, the disc placed just below the point where intravenous therapy tube was positioned (Figure 2, position 2), indicating the absence of caffeine molecules, and thus the efficiency of the ISATI.

Figure 4 presents the ¹H-NMR spectra analysis of sensor discs following a 6-h mechanical ventilation simulation with a caffeine solution sprayed at 120-min intervals inside the ISATI. Caffeine molecules were not found on any of the sensor discs except position 4 (spectrum E), the control sensor located inside the ISATI.

After determining the isolation efficacy of the ISATI through ¹H NMR analysis using caffeine as a molecular marker, we next evaluated its efficacy using synthetic viral particles to better emulate a clinical scenario involving infected patients.

Figure 5(a) illustrates that undetectable levels of synthetic viral RNA (10⁷ SARS-CoV-2 RNA copies/mL) were found in samples collected from the external environment of the ISATI following simulated aerosolization experiments. The N gene of the synthetic viral RNA was only detected in samples collected from positions inside the ISATI, identified as number 10 (internal surface #2, the inner surface of the plastic cover), position 11 (manikin) and 12 (HEPA filter, the air inflow side of the microparticle filter used to connect to the hospital vacuum system, located inside the ISATI). The RdRp gene was also only detected in the samples collected from inside the contaminated ISATI environment, at positions 11 and 12 (Figure 5(a)).

To simulate a more extreme viral particle concentration environment, the E gene (10¹⁰ synthetic SARS-CoV-2 viral RNA per mL, 15 mL of solution) was found to be detectable in all analyzed samples. Here a scattering gradient was observed, with much higher concentrations identified inside the ISATI with gradually reduced levels found in the external environment (Figure 5(b)).

4. Discussion

Experimental testing under all simulated conditions indicated that ISATI effectively contained the molecular marker evaluated, 1 ppm of caffeine, without leading to contamination in the surrounding external environment during and after the



Figure 3. 1H-NMR spectra readings following NIV with CPAP simulations. (a) 0.001% caffeine in D2O solution. Extract from nitrocellulose sensor discs positioned at: (b) entrance of multiparameter patient monitoring cables and respiratory tubes (Figure 2, position 1); (c) entrance of intravenous therapy tube (Figure 2, position 3); (d) inside the ISATI (Figure 2, position 4).



Figure 4. 1H-NMR spectra readings following 6-hour period of simulated mechanical ventilation. (a) 0.001% caffeine in in D2O solution. Extract from nitrocellulose sensor discs positioned at: (b) entrance of multiparameter patient monitoring cables and respiratory tubes (Figure 2, position 1); (c) entrance of intravenous therapy tube (Figure 1, position 2); (d) on a health professional's chest (Figure 2, position 3); (e) inside the ISATI (Figure 2, position 4).

performed simulations, as determined by ¹H-NMR analysis of sensor discs.

The simulated conditions in this study were designed to be more critical than actual medical situations. For 900 minutes in the simulations, the caffeine solution was aerosolized under high pressure (average pressure of 200 psi), equivalent to approximately 14,000 cm H₂O, which is much higher than that used in NIV with CPAP (max. 30 cm H₂O). All experimental simulations resulted in the internal environment of ISATI becoming saturated with the aerosolized solution, with clearly visible droplet formation inside the plastic cover. Experimental simulations also involved concentrations of synthetic RNA particles aerosolized inside the ISATI that simulated much more infectious conditions than the virus concentrations described in clinical settings [4,9,16]. The aerosolization of Synthetic RNA virus at a concentration of 10⁷ copies/mL was equivalent to 150 million virus particles, considering that 15 mL of solution was aerosolized inside ISATI. It simulated a condition with extremely high virus air concentrations, not identified in publications describing virus air concentrations in clinical settings [4,9]. The concentration of 10¹⁰ synthetic RNA copies/mL aerosolized 150 billion viral particles in 15 mL of solution, simulating an inconceivable



Figure 5. Evaluation of occupational and environmental contamination by RT-PCR amplification of synthetic SARS-CoV-2 RNA. (a) Detection of 107 copies/mL of synthetic SARS-CoV-2 RNA by RT-PCR: genes N and RdRP. (b) Detection of 1010 copies/mL of synthetic SARS-CoV-2 RNA by RT-qPCR: gene E. Ct* values for each tested sample are represented as heatmaps (left side) or scatter plots (right side). ND = not detected after 45 amplification cycles. Locations of swab samples for RT-qPCR analysis: HEPA filter: air inflow position on the microparticle filter used for air removal, inside ISATI; manikin, inside ISATI; internal surface #1 and #2: inner surface of the plastic cover, inside ISATI; tube: exit position of the internal tube to connect ISATI to hospital vacuum system; lab coat #1 and #2: external surface of health professional's disposable gown, following disassembly of ISATI; external surface #1 and #2: outer surface of plastic cover, outside ISATI; window: internal surface of hospital room window; Vacuum: inner part of the hospital vacuum flask, connected to ISATI air suction assembly; table: table next to hospital bed where simulations occurred. *Ct = Cycle threshold, i.e. number of amplification cycles in which fluorescence levels exceeds background threshold, being inversely proportional to the amount of virus nucleic acid present in the sample.

clinical condition not described in scientific publications in the context of respiratory airborne virus conditions [4,9,16]. This extreme viral particle concentration was intentionally used to certify that small amounts of synthetic virus particles could be detected outside the ISATI, and was not designed to evaluate the system's efficacy.

Sars-CoV-2 concentrations in throat and sputum samples of infected patients have reportedly ranged from 641 copies per mL to 1.34×10^{11} copies per mL, with a median of 7.99×10^4 /mL in throat samples and 7.52×10^5 /mL in sputum samples [15]. Studies identify lower environmental concentrations of SARS-CoV-2 particles than levels found in infected patients' throats and saliva [4,9,16]. Studies have also indicated that airborne virus concentrations near hospitalized COVID-19 patients present maximum concentrations of 4.82×10^4 /mL in the air next to patients receiving oxygen by nasal cannula

[4,9]. Mean air virus concentrations in patient rooms had the highest values at 2.86×10^3 /mL [4].

SARS-CoV-1 infected patients were reported to present saliva concentrations of 7.08 × 10³ to 6.38 × 10⁸ copies per mL (median: 9.92 × 10⁴ copies/mL) [17]. Data on SARS-CoV-1 nasopharyngeal concentrations ranges from 1.7x10³/mL to 3.4x10⁷/mL [17,18]. Airborne SARS-CoV-1 concentrations near infected patients ranged from 1.1 × 10¹ to 1.3 × 10⁵ copies/mL [19]. The number of SARS-CoV-1 particles expelled per cough in infected patients was shown to be less than that found in nasopharynx [18–20]. SARS-CoV-1 cough concentrations ranged from 900 particles to 3.02×10^5 particles/mL/cough [20].

Average air concentrations of viral load in influenza were found to be 4×10^5 copies/mL up to 0.3 m away from infected patients, while higher numbers of particles (1.9×10^6) were identified closer to patients [21].

Published data on virus concentrations in the air near infected patients with influenza virus, SARS-CoV-1 and Sars-CoV-2 indicate that total viral concentrations do not exceed 10⁶ particles/mL even in the presence of aerosol-producing medical procedures [4,9,19–21]. These data confirm that the synthetic virus concentration used in the present study (10⁷ copies/mL) to evaluate the efficacy of the ISATI is considerably higher than the expected air concentrations found near patients infected with respiratory viruses [4,9,19–21].

Airborne viral concentrations of SARS-CoV-1 and Sars-CoV-2 have been reported to be similar [4,9,19,20]. Considering the concentration of synthetic RNA particles used in the present experimental simulations (10⁷ copies/mL, equivalent to 150 million viral particles) compared to the maximum reported concentration of SARS-CoV-1 per cough (30.2x10⁴ particles/mL/cough) [20], an equivalent measure would be a patient coughing no less than 496 times in 60 min period in order to achieve the virus concentration established in the present study.

Considering all experimental simulations conducted herein, a total of 160 external sensor discs were analyzed, with no caffeine detected on any of the external sensors analyzed. In addition, synthetic SARS-CoV-2 RNA particles were used as an additional method of evaluating the ability of ISATI to isolate virus particles and protect the surrounding environment. The efficacy of the ISATI was confirmed by the detection and quantification of synthetic RNA by RT-PCR amplification.

The molecular size of caffeine is on the order of Angstroms (10^{-10}m) , while viral particles are measured in nanometers (10^{-9}m) . Importantly, SARS-CoV-2 dissemination occurs through the aerosolization of larger particles measuring in submicrons (0.25 to 1.0 µm) or supermicrons (>2.5 µm) [9]. It follows that ISATI was shown to inhibit the dissemination of caffeine molecules, which are smaller than viral particles, and also to prevent the spread of larger-sized synthetic SARS-CoV -2 RNA. Regardless of the size of the marker used in experimentation, our results indicate the environmental safety of ISATI as an isolation system capable of proving occupational protection to health professionals treating patients with aero-sol-transmitted infections.

The data in the literature are controversial regarding the use of CPAP in the treatment of virus-related respiratory failure. Publications indicate that this procedure does not decrease the need for intubation and should be avoided due to high failure rates in patients with acute respiratory distress syndrome and H1N1 [12,22]. However, clinical reports have also indicated that patients affected by acute respiratory syndrome during the 2003 (SARS) and 2009 (H1N1 virus) epidemics who were submitted to CPAP had shorter hospital stays and lower mortality rates than patients treated with mechanical ventilation, obtaining results similar to hospitalized patients who did not need ventilation support [23,24], with a CPAP effectiveness rate of 40.6% [24]. Benefits with regard to NIV also reveal that similar rates of mortality were found in patients for whom CPAP support was ineffective, thus requiring further mechanical ventilation, as those necessitating intubation as the initial treatment of acute respiratory failure [23,24]. Guidelines have been published suggesting the use of CPAP and HFNO [25,26] and publications

provide evidence of benefits of these therapies in COVID-19 patients [27–29].

Regardless of the controversy as to whether early intubation, CPAP or HFNO represent the best initial treatment option for respiratory virus-related hypoxemia, it is important to recognize that ICU availability has been lacking in some countries during the COVID-19 pandemic, thus necessitating alternative measures for the mechanical ventilation of hypoxemic patients, even if performed as a temporary stopgap measure. Insufficient amounts of ICU beds during respiratory viral outbreaks can lead to the collapse of health systems, and NIV could offer a solution to provide oxygen to patients, thus keeping them alive, until achieving stability in ICU capacity. However, the conduct of NIV in the context of aerosol-transmitted infections must be performed in hospital environments that can ensure occupational safety for health-care professionals.

Considering the experimental data presented herein, we conclude that ISATI represents an efficient system to prevent the dissemination of microparticles under the simulated conditions described. ISATI could be a useful tool to boost occupational and environmental safety in cases where NIV or HFNO are indicated for hypoxemic patients with respiratory viral infections, dispensing the need to isolate these patients exclusively in laminar airflow and negative pressure environs. The system can also be used to promote environmental protection by isolating infected patients under mechanical ventilation for up to 6 hours, and offers protection to health-care professionals by lowering airborne contamination within hospitals.

The results of this experimental study provide convincing evidence of ISATI's efficacy in the simulations described in this publication. Considering the demands placed by the Sars-CoV -2 pandemic on the Brazilian health system, the clinical use of ISATI was approved by national health authorities under the brand of BhioCOVID[®], manufactured by Bhiosupply[®].

The process required to assemble ISATI is simple and can be accomplished in just a few minutes. With the patient lying on a hospital bed, the non-disposable stainless steel components are installed. Part of this structure houses the microparticle filter connected to a plastic tube that is attached to the hospital's vacuum system, establishing an air suction system once activated. A CPAP face mask or nasal catheter for HFNO are attached to the patient. The plastic cover is then positioned over the patient and the hospital bed. An elastic band secures the inferior part of the plastic cover to the hospital bed. Oxygen flow for CPAP or HFNO is then initiated.

As ISATI resembles a chamber, CO_2 buildup represents a plausible concern. However, as the patients inside are being treated with oxygen, high oxygen concentrations are produced. In addition, ISATI does not constitute a fully enclosed chamber; rather, it promotes isolation. The air under the plastic cover is continuously aspirated, thereby creating a preferential airflow. The elastic band that fixes the inferior part of the plastic cover to the bed has been intentionally designed to allow air to enter, which results in the establishment of a negative pressure environment. Our experiments demonstrate that the air inside the ISATI does not exit the chamber through its inferior section, as no markers were detected by sensors/sample collection. The plastic that covers the entire hospital bed is transparent. There have been no COVID-19 infected patients reports of feelings of claustrophobia, in clinical settings, when treated with CPAP or HFNO using ISATI.

Once noninvasive ventilation is started, provoking aerosolized particle dissemination, lifting the plastic cover of ISATI's chamber to access to the patient is inadvisable, as this would promote contamination. If there is any need to gain access to the patient, the entire plastic cover with its disposable items would need to be completely discarded.

Removal of the plastic cover can be accomplished in seconds. Oxygen flow is first turned off or lowered to 2 L per minute, after which the elastic band underneath the cover is removed. Two health personnel positioned on the sides of the bed remove the plastic cover by rolling it up with the external surface outward for eventual disposal. The microparticle filter and air suction tube are also retrieved and discarded. All non-disposable items are cleaned with antiseptic solutions in the case of reuse by the same patient. Nondisposable items, such as the stainless steel structure, are autoclaved prior to being used for another patient.

Our experimental tests did not detect any occupational risk in the removal and discard of the plastic cover when the suction system remained connected to the microparticle filter under aspiration. Swabbing to identify synthetic virus particles and sensors for the detection of caffeine placed on the garments of the personnel who removed the plastic cover did not reveal the presence of any markers.

5. Conclusions

The present experiments indicate that ISATI is effective in microparticle containment under simulated conditions of CPAP, HFNO and mechanical ventilation. In all simulation scenarios, the molecular marker aerosolized inside the ISATI was undetectable at the exterior sampling positions evaluated. The use of a synthetic SARS-CoV-2 RNA gradient both inside and outside the ISATI demonstrated its efficacy in viral isolation capability. This tool should be considered in an effort to guarantee the environmental and occupational safety of health professionals when performing CPAP and HFNO in eligible respiratory virus-infected patients to diminish the risk of contamination.

6. Expert opinion

The development of the ISATI, presented in this manuscript, was only possible through the partnership between Brazilian universities, research institutions and the industry. The process started in March 2020 and took place during the peak of COVID-19 cases in Brazil. It required the commitment of the researchers who needed to travel three times, a distance of 1,600 Km, to conduct the validation tests presented in this manuscript. The objective was to obtain an isolation system that would allow the use of noninvasive ventilation or HFNO in COVID-19 hypoxemic patients, ensuring occupational and environmental safety against aerosol contaminated with SARS-CoV-2. Safety in the isolation of viral particles was the main objective, but the isolation system also needed to be easy to

handle, to be widely available and to be possible to use in any hospital, especially in the less complex ones. All of these goals have been achieved. The results of the preclinical validation tests described here secured approval for clinical use of ISATI by the Brazilian National Health Surveillance Agency (ANVISA). ISATI started to be produced under the brand name of BhioCOVID® and used in clinical practice in Brazil. In the beginning of the pandemic, guidelines in Brazil indicated to proceed with early orotracheal intubation in cases of moderate hypoxia. Initially, the offer of noninvasive ventilation intended to be an emergency alternative of offering oxygen to hypoxemic COVID-19 patients, in view of the imminent lack of ICU beds. BhioCOVID® could guarantee the emergency supply of oxygen through noninvasive ventilation until ICU vacancies were available. But with the clinical use of BhioCOVID®, allowing the offer of CPAP and HFNO, it could be observed that several patients with COVID-19 who initially had hypoxia and criteria for orotracheal intubation, did not need to undergo mechanical ventilation through the adoption of CPAP sessions or continuous use of HFNO. This was a great benefit to these patients, as they were able to overcome the hypoxia caused by COVID-19 without requiring mechanical ventilation, avoiding the consequences that can result from a prolonged induced coma. In addition to reducing the hospital costs of treating these patients. The greatest proof of BhioCOVID®'s effectiveness was the success of its use in clinical practice. It is an easy-to-use tool that allows delivery of CPAP and HFNO in patients with respiratory infections transmitted by aerosol, with occupational safety, without requiring patients to be in isolated rooms with negative pressure. It can be a simple alternative to deliver CPAP, HFNO or permit the use of nebulization treatments during the COVID-19 pandemic or in other aerosol transmitted respiratory infections.

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Authorship contributions

Authors that participated in the process of planning, conception of the study design, conducting experiments, acquisition, interpretation and analysis of data: Quadros CA, Leal MCBDM, Baptista-Sobrinho CDA, Nonaka CK, Souza BS, Ferreira AG. Authors that participated in conducting experiments and data acquisition: Milan-Mattos JC, Catai AM, Pires Di Lorenzo VA. All authors participated in writing the manuscript.

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Conflict of interest statement

The authors deny the existence of any conflicts of interest.

Declaration of interest

The authors have no other relevant affiliations or financial involvement with any organization or entity with a financial interest in or financial conflict with the subject matter or materials discussed in the manuscript apart from those disclosed.

Data sharing

The data, analytic methods, and study materials will be made available to other researchers by request to the corresponding author.

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